Flow injection analysis of paracetamol using a biomimetic sensor as a sensitive and selective amperometric detector

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This work describes the coupling of a biomimetic sensor to a flow injection system for the sensitive determination of paracetamol. The sensor was prepared as previously described in the literature (M. D. P. T. Sotomayor, A. Sigoli, M. R. V. Lanza, A. A. Tanaka and L. T. Kubota, J. Braz. Chem. Soc., 2008, 19, 734) by modifying a glassy carbon electrode surface with a Nafion[®] membrane doped with iron tetrapyridinoporphyrazine (FeTPyPz), a biomimetic catalyst of the P450 enzyme. The performance of the sensor for paracetamol detection was investigated and optimized in a flow injection system (FIA) using a wall jet electrochemical cell. Under optimized conditions a wide linear response range (1.0 \times 10^{-5} to 5.0×10^{-2} mol L⁻¹) was obtained, with a sensitivity of 2579 (\pm 129) µA L µmol⁻¹. The detection and quantification limits of the sensor for paracetamol in the FIA system were 1.0 and 3.5 μ mol L⁻¹, respectively. The analytical frequency was 51 samples h^{-1} , and over a period of five days (320 determinations) the biosensor maintained practically the same response. The system was successfully applied to paracetamol quantification in seven pharmaceutical formulations and in water samples from six rivers in São Paulo State, Brazil. PAPER

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Introduction

Pharmaceutical substances and personal care products have recently been recognized as an important class of organic pollutants due to their physical–chemical properties, which allow their persistence and bioaccumulation in the environment, provoking negative effects in aquatic or terrestrial ecosystems at concentrations as low as a few nanograms per liter. $1-3$

Many studies have reported the presence of a large number of pharmaceuticals, such as anti-inflammatories, analgesics, bblockers, lipid regulators, antibiotics, anti-epileptics and estrogens, at average concentrations in the μ g L⁻¹ range, in sewage treatment plant effluents, surface and groundwater and even in drinking water, $4-9$ indicating their poor degradability in sewage treatment plants.^{5,8,9}

Concern about pharmaceuticals has often focused on antibiotics, which may promote resistance in natural bacterial populations, and on hormones, which may induce estrogenic responses as well as alterations in the reproduction or development of aquatic organisms.^{1,2,10,11} Wastewaters are the main disposal route of pharmaceuticals into the environment. Nevertheless, other different sources of pharmaceutical release can be proposed to explain the appearance of these xenobiotics in waters and soils, such as inadequate treatment of manufacturing waste, direct disposal of unconsumed drugs in households and

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the use of manure for topsoil dressing.1,4,5,10 These compounds are considered as a new category of persistent pollutants.³

There is therefore interest in the development of simple, sensitive, selective and reliable methods for the determination of these chemicals, not only in the aquatic environment, but also during production of pharmaceuticals and in dissolution studies.¹²

Paracetamol (acetaminophen, N-acetyl-p-aminophenol, 4-acetamidophenol or tylenol) is included in this new class of environments pollutants. It is widely used for young children, old people, and in pregnancy as an antipyretic and analgesic drug, to control mild to moderate pain or reduce fever. Its action is similar to that of aspirin, so it is an appropriate alternative for patients who are sensitive to acetylsalicylic acid.¹³

Thus, it is very important to establish fast, simple and accurate methodologies for the detection of paracetamol in quality control analyses (in pharmaceutical formulations), for medical control (in biological fluids such as urine, blood or plasma) and more recently for application in environment control in samples from sewage treatment plant effluents, surface and groundwater and even in drinking water.¹⁴ It is known that overdose ingestions of acetaminophen can lead to accumulation of toxic metabolites, which may cause severe and sometimes fatal hepatotoxicity and nephrotoxicity.15–17

Many analytical methodologies, using both batch and flow modes, have been proposed for the determination of paracetamol, including titrimetry,¹⁸ spectrophotometry (spectrofluorimetry, near infrared reflectance spectrometry, Raman spectrometry and Fourier transform infrared spectrophotometry),^{19–26} chromatography,^{27,28} chemiluminescence^{29–31} and enzymatic analysis.^{32,33} Electrochemical methods^{34–36} are an attractive alternative, since they are fast, inexpensive, and can be adapted for portable, disposable and miniaturized applications.

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Paracetamol can be readily oxidized at carbon paste or glassy carbon electrodes,³⁷ however these amperometric procedures are non-selective, since the potential involved in this process ranges from 0.6 to 0.8 V, and various substances are electroactive in this potential interval. However, use of modified electrodes, such as biosensors $32,37$ and more recently biomimetic sensors, 38 can enable operation at potentials much lower than those normally used, thus decreasing the interference.³⁷

Flow injection analysis (FIA) has been routinely used since its inception to provide automated control of sample handling.³⁹ FIA involves the injection of a reproducible sample volume into a continuously flowing carrier solution, followed by quantification at a detector device. In addition to automated control, FIA offers other advantages including convective mass transport, matrix exchange and increased precision. The combination of FIA with electrochemical and selective sensors is an attractive tool because of the flexibility of the former and the diagnostic power of the latter.⁴⁰ Flow-through electrochemical sensors allow the continuous real-time monitoring of analytes, and are among the most important types of analytical tools that have received extensive attention, in pharmaceutical analysis as well as in other environmental and biochemical applications.13,37,40,41 Pursectannel can be result) evolvined at carbon past or giany

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This paper reports on the development of the first (as far as we are aware) biomimetic sensor coupled to a FIA system for analysis of paracetamol in pharmaceutical formulations and aquatic samples.

Experimental

Chemicals and solutions

All chemicals used in the construction and application of the sensor were analytical grade reagents. All chemicals used in the chromatographic experiments were high performance liquid chromatography (HPLC) grade reagents.

The biomimetic complex, iron(III) tetrapyridinoporphyrazine (FeTPyPz), was prepared and purified as previously described.⁴²

Acetic acid and N,N–dimethylformamide (DMF) were acquired from Synth (São Paulo, Brazil). Paracetamol (acetaminophen) was obtained from Sigma (St. Louis, USA). 5% (m/v) Nafion[®] solution was from Aldrich (Milwaukee, USA). Sodium acetate was acquired from Merck (Darmstadt, Germany), and all HPLC grade solvents were from Tedia (Rio de Janeiro, Brazil).

Paracetamol and acetate buffer solutions were prepared with water purified in a Millipore Milli-Q system, and the pH was determined using an Orion® pH meter (Model 3 Star pH).

Biomimetic sensor construction

The biomimetic sensor was constructed as previously described.³⁸ First, a solution containing 5 mg mL⁻¹ of the FeTPyPz in DMF was prepared. Then, the surface of a glassy carbon (GC) electrode (Metrohm®, Switzerland), with a geometrical area of 0.126 cm², was cleaned according to the procedure described in the literature.⁴³ After cleaning the electrode, $100 \mu L$ of FeTPyPz solution was mixed with 50 μ L of 5% (m/v) Nafion® solution, and an aliquot of 50 μ L of this mixture placed on the surface of the electrode. Finally, the solvent was evaporated at room temperature during 6 h, forming a thin green film.

Flow manifold and electrochemical measurements

The biomimetic sensor was inserted into a flow-through wall-jet amperometric cell and used as the working electrode (Fig. 1). An $Ag|AgCl(KCl_{sat})$ electrode was the reference, and a platinum wire was the auxiliary electrode. The electrodes were connected to a potentiostat (Palm-sense®, Palm Instruments BV, The Netherlands) interfaced to a microcomputer for potential control and data acquisition.

A peristaltic pump (Ismatec[®]) was used to provide the flow of the 0.1 mol L^{-1} (pH 3.6) acetate buffer carrier solution. The standards and samples containing paracetamol were injected into the carrier using a sliding central bar sampling valve.⁴⁴

HPLC analysis

In order to validate the results obtained using the proposed sensor, they were compared to those obtained using a chromatographic method based on HPLC.⁴⁵ Chromatographic analyses were performed using a Shimadzu® Model 20A liquid chromatograph coupled to an UV/Vis detector (SPD-20A), autosampler (SIL-20A) and a degasser DGU-20A5, controlled by a personal computer. A C18 column (250×4.6 mm, Shim-Pack CLC–ODS) was used, inside an oven (Shimadzu® CTO– 10AS) maintained at 30 $^{\circ}$ C. The mobile phase was a mixture of methanol and water in a ratio of 13 : 87 (v/v). The flow rate was 1.0 mL min⁻¹, the sample injection volume 20 μ L, and the detector absorption wavelength 254 nm.

Pharmaceutical formulation analysis

Quantification of paracetamol in seven commercial samples was carried out according to the external standards method. Samples of four commercial solutions were analyzed after simple dilution with deionized water, without additional treatment. These were: Paracetamol (Ache®, Lot L0804193, validity 08/10), labeled value of 200 g L^{-1} (1.32 mol L^{-1} paracetamol); Tylenol[®] for children (Janssen-Cilag, Lot LFL169, 04/10), fruit flavor with labeled value of 160 mg of paracetamol for each 5 mL of syrup; Tylenol® in drops (Janssen-Cilag, Lot FL121, 04/11), labeled value of 200 g L^{-1} ; Tylenol® for babies, concentrated oral

Fig. 1 Schematic diagram of the flow injection system for amperometric determination of paracetamol. L: sample loop $(75 \mu L)$; WE: working electrode (biomimetic sensor); AE: auxiliary electrode (platinum); RE: home-made Ag|AgCl(KCl_{sat} reference electrode).

suspension (Janssen-Cilag, LAL008, 11/09), fruit flavor with labeled value of 100 g L^{-1} of paracetamol. Three additional samples of tablets were also analyzed: Tylenol® DC (Janssen-Cilag, Lot LCL008, 01/11), labeled value per tablet of 500 mg of paracetamol and 65 mg of caffeine; Tylenol® AP (Janssen-Cilag, Lot LFL105, 02/10), labeled value per tablet of 650 mg of paracetamol; Paracetamol (EMS®, Lot L15655, 05/10), labeled value of 750 mg of paracetamol per tablet.

Aquatic sample analysis

Six water samples from rivers in São Paulo State, Brazil, were enriched with paracetamol and then analyzed using the proposed sensor in order to evaluate the matrix effect on recovery values.

Results and discussion

Biomimetic sensor for paracetamol

The optimization and performance, in batch mode, of the biomimetic sensor used in this work has been reported previously.³⁸ Table 1 provides the characteristics of this sensor, where the FeTPyPz complex acts as a biomimetic catalyst of the P450 enzyme.⁴⁶

The sensitivity, operational stability and response time shown by the sensor in batch mode indicated that the device should be able to be satisfactorily coupled to a flow system. Thus, in the next step the sensor was installed in a FIA system shown in Fig. 1. An advantage of flow conditions is that the electrochemical products are more efficiently removed from the electrode surface, avoiding poisoning of the sensor and increasing its lifetime.⁴⁷ Further experiments, using the FIA system, were performed in order to optimize parameters including flow rate, injected sample volume (V_i) and applied potential.

Table 1 Analytical and kinetic parameters obtained for paracetamol determination using the biomimetic sensor based on the FeTPyPz catalyst in the batch mode.³⁸

Parameter	Response
Linear range/mol L^{-1}	4.0×10^{-6} to 4.2×10^{-4}
Sensitivity/ μ A L mol ⁻¹	$5798 + 73$
Correlation coefficient	0.9994 $(n = 10)$
Detection limit/ μ mol L ⁻¹	12
Quantification limit/ μ mol L^{-1}	4.0
Measurement repeatability $(RSDa)$, $n = 7$ and [Paracetamol] = 2.4 \times 10^{-4} mol L^{-1})	3.4
Reproducibility in the construction of the sensors $(RSD^a, n = 4)$	5.0
Applied potential [mV vs.] Ag[AgCl(KCl _{sat})]	450
Response time/s	0.5
Sensor lifetime/days	180
Operational stability/ measurements	50 (kept 95% of the initial signal)
Paracetamol diffusion coefficient/ $\rm cm^2~s^{-1}$	1.066×10^{-6}
Apparent Michaelis-Menten constant $(K_{\text{WIM}}^{\text{app}})/\text{mol} \ L^{-1}$	2.15×10^{-2} mol L ⁻¹
α RSD: relative standard deviation.	

FIA system optimization

Optimization of the applied potential was necessary because a home-made $Ag|AgCl(KCl_{sat})$ reference electrode was used in the wall jet cell. Fig. 2 shows the results obtained under flow conditions. The maximum response of the sensor was achieved at an applied potential of 500 mV, thus this potential was selected during subsequent experiments. Although, in the batch system,¹ higher sensitivity was obtained at 450 mV vs. a commercial $Ag|AgCl(KCl_{sat})$ electrode (Table 1), under flow conditions a small increment of +50 mV was observed.

The flow rate dependence of the signal response of the biomimetic sensor can be seen in Fig. 3. The signal response for paracetamol increases up to a flow rate of 1.25 mL min⁻¹ because mass transfer, accompanied by electronic transfer, increases with increasing flow rate. The subsequent decrease in the signal response with increased flow rate is due to limitations of the chemical reaction, since as the sample passes through the electrode faster, the fraction of the substrate oxidized by its chemical reaction with the FeTPyPz is smaller. This behavior can be explained considering the short response time (0.5 s), and the

Fig. 2 Influence of the applied potential on the response to 1.0×10^{-4} mol L^{-1} paracetamol, with V_i of 75 µL, flow rate of 1.25 mL min⁻¹ and using a 0.1 mol L^{-1} acetate buffer at pH 3.6 as carrier. The error bars correspond to the standard deviation for seven replicates.

Fig. 3 Effect of the flow rate on the response to 1.0×10^{-4} mol L⁻¹ paracetamol, with V_i of 75 µL, and using a 0.1 mol L⁻¹ acetate buffer at pH 3.6 as carrier. The error bars correspond to the standard deviation for seven replicates.

Fig. 4 Effect of injected sample volume (V_i) on the response to 4.0 \times 10^{-4} mol L⁻¹ paracetamol. The experiments were carried out with 0.1 mol L^{-1} acetate buffer at pH 3.6 as carrier, with a flow rate of 1.25 mL min⁻¹ and applying a potential of 500 mV vs. Ag|AgCl. The error bars correspond to the standard deviation for seven replicates.

response mechanism of the sensor to be characteristic of a typical catalytic electro-oxidation (chemical/electrochemical).38,48 Therefore an optimized flow rate of 1.25 mL min⁻¹ was used.

The effect of the injected sample volume (V_i) on the sensor response was studied. The signal response (Fig. 4) increased with increasing V_i , perhaps related to a longer sample contact time with the catalytic zone of the biomimetic sensor. However, at higher sample volume a lower analytical frequency and lower measurement repeatability were obtained; as evaluated by the standard deviation for seven replicates. A V_i of 75 μ L was therefore selected, on the basis of better repeatability.

Analytical characteristics of the proposed FIA system

Fig. 5 presents the FIA signals as a function of paracetamol concentration under optimized conditions, and it can be

Fig. 5 FIA signals obtained for a biomimetic sensor under flow conditions for different paracetamol analyses. Experimental conditions: $V_i =$ 75 µL, 0.1 mol L^{-1} acetate buffer at pH 3.6 (1.25 mL min⁻¹) and applied potential of 500 mV vs. Ag|AgCl. [Paracetamol]: $a = 1.0 \times 10^{-5}$ mol L⁻¹; $b = 5.0 \times 10^{-5}$ mol L^{-1} ; $c = 1.0 \times 10^{-4}$ mol L^{-1} ; $d = 5.0 \times 10^{-4}$ mol L^{-1} ; $e = 1.0 \times 10^{-3}$ mol L^{-1} ; $f = 5.0 \times 10^{-3}$ mol L^{-1} ; $g = 1.0 \times 10^{-2}$ mol L^{-1} ; $h = 2.5 \times 10^{-2}$ mol L^{-1} ; $i = 5.0 \times 10^{-2}$ mol L^{-1} .

Fig. 6 Relative response obtained for 1.0×10^{-3} mol L⁻¹ paracetamol at an applied potential of 500 mV vs. Ag A gCl, as a function of the number of assays. (a) Conditioning of the system. Each point corresponds to an average of eight injections.

observed that there is no memory effect for the sensor response. The analytical curve obtained from the data in Fig. 5 showed a wide linear response range, from 1.0×10^{-5} to 5.0×10^{-2} mol L^{-1} , described by

$$
\Delta i = 2702 \ (\pm 77)
$$
 [Paracetamol] + 0.02 (\pm 0.01) (Eq. 1)

with a correlation coefficient of 0.9997 ($n = 9$), where the current variation, Δi , is given in μA and the paracetamol concentration [Paracetamol] in mol L^{-1} . It is important to emphasize that the linear response range shown by the proposed system is wider than that of other FIA systems reported in the literature, where spectroanalytical $41,49-51$ or electroanalytical $14,32$ methods were employed.

Detection and quantification limits, determined from the standard deviation of ten independent measurements of the blank in accordance with IUPAC recommendations,⁵² were 1.04×10^{-6} mol L⁻¹ and 3.46×10^{-6} mol L⁻¹, respectively. The

Table 2 FIA system analytical parameters obtained for paracetamol determination using the biomimetic sensor based on the FeTPyPz catalyst

Parameter	Response
Applied potential vs.	0.5V
Ag AgCl(KCl _{sat})	
Flow rate/mL min ⁻¹	1.25
V_i/uL	75
Linear range/mol L^{-1}	$1.0 \times 10^{-5} - 5.0 \times 10^{-2}$
Sensitivity/ μ A L μ mol ⁻¹	$2579 + 129$
Ouantification limit/ μ mol L ⁻¹	35
Detection limit/ μ mol L^{-1}	1 ₀
Measurement repeatability (RSD, n	1.2%
$= 7$ and [Paracetamol] $= 4.0 \times$	
10^{-4} mol L^{-1})	
Reproducibility in the construction	5.0%
of the sensors (RSD, $n = 3$)	
Operational stability	320 measurements or 5 days (kept)
	93% of the initial signal)
Analytical frequency	51 samples h^{-1}

Table 3 Determination of paracetamol in pharmaceutical formulations using the proposed FIA system, and the chromatographic method as reference

		Experimental value		
Sample	Label value	Comparative method (HPLC)	Proposed sensor	Error $(\%)$
Tylenol [®] (LFL121, 04/11)	$200 \text{ mg} \text{ mL}^{-1}$	190	196	$+3.2$
Paracetamol (L0804193, 08/10)	$200 \text{ mg } \text{mL}^{-1}$	197	203	$+3.0$
Tylenol [®] (LFL169, 04/10)	160 mg/5 mL	162	163	$+0.6$
Tylenol [®] (LAL008, 11/09)	$100 \text{ mg } \text{m} \text{L}^{-1}$	92	96	$+4.3$
Tylenol DC (LCL008, 01/11)	500 mg/tablet	500	488	-2.4
Tylenol AP (LFL105, 02/10)	650 mg/tablet	656	680	$+3.6$
Paracetamol (L15655, 05/10)	750 mg/tablet	765	800	$+4.6$
Under these conditions, the biosensor can be operated with an analytical frequency of 51 injections h^{-1} . The FIA system reproducibility was evaluated by comparison of the sensitivities obtained using three sensors prepared on different days. The RSD value obtained was 5.0%, the same as that obtained for the sensor in batch mode.		Application	sensor for determination of paracetamol in pharmaceutical formulations, and in environmental and industrial samples. The application of the proposed sensor was tested in a similar	
Finally, Fig. 6 shows the operational stability of the sensor under flow conditions. This parameter was investigated using eight consecutive injections of 1.0×10^{-3} mol L ⁻¹ paracetamol		way to the batch mode, ³⁸ using two different sample types. The first type, the commonest, were the seven commercial formula- tions. The second type were the river water samples, which were		
standard solution, every 30 min for 4 h each day, over a 5 day			enriched with paracetamol at two levels of concentration in order	
period, totaling 64 injections per day or 320 injections over the			to demonstrate the applicability of the proposed FIA system to	
5 days of the evaluation. During this time the sensor presented		environmental samples.		
			Table 3 shows the results obtained for the determination of	
the same response.	The flow was maintained during periods when no injection was		paracetamol in the commercial formulations. The concentrations	
carried out, in order to evaluate the resistance of the film on the			were determined by the FIA system using the external calibration	
electrode surface. After 5 days the film was still firmly adhered to the electrode surface with no change in its annearance. This is			method, and compared with those obtained with the official chromatographic method. The results were not significantly	

The flow was maintained during periods when no injection was carried out, in order to evaluate the resistance of the film on the electrode surface. After 5 days the film was still firmly adhered to the electrode surface, with no change in its appearance. This is

Fig. 7 FIA responses obtained for the sensor calibration and for measurements of the six river waters enriched with paracetamol at two levels of concentration. A–F: 5.0×10^{-2} mol L⁻¹ paracetamol; A'–F': 1.0 \times 10⁻⁴ mol L⁻¹ paracetamol. A and A': Tietê river at the Usina da Barra club; B and B': Tietê river on the outskirts of Igaraçu city; C and C': Tietê river by the bridge in Barra Bonita city; D and D': Jacaré Guaçú; E and E': Jacaré Pepira; F and F': Jaú. [Paracetamol]: the same as a-i in Fig. 5.

Application

Table 3 shows the results obtained for the determination of paracetamol in the commercial formulations. The concentrations were determined by the FIA system using the external calibration method, and compared with those obtained with the official chromatographic method. The results were not significantly different, at a confidence level of 95%, suggesting that the proposed methodology is an efficient and rapid alternative for paracetamol analyses.

Fig. 7 shows the response profile obtained for analyses of the six river water samples enriched with paracetamol at two concentration levels. It can be seen in Table 4 that very good recoveries were obtained, with values close to 100% and near those obtained with the HPLC method.

Table 4 Recovery values obtained with the proposed FIA system for paracetamol in water from rivers

	% Recovery		
River	FIA ^a	HPLC	
Jacaré Pepira	$100.0 + 2.0$	96	
Jacaré Guacú	$96.4 + 3.6$	94	
Jaú	$99.8 + 1.3$	96	
<i>Tietê</i> river on the outskirts of <i>Igaracu</i> city	$97.8 + 1.9$	94	
<i>Tietê</i> river by the bridge in <i>Barra</i> Bonita city	$96.9 + 0.5$	94	
Tietê river at the Usina da Barra club	$95.8 + 5.6$	92	

 a^a Average of recovery values for the two concentration levels.

Conclusions

This work describes for the first time the determination of paracetamol using a biomimetic sensor as a sensitive and selective detector within a flow injection system. The FIA arrangement presents a wide response range and high sensitivity, and was satisfactorily applied to the analysis of commercial pharmaceutical formulations. It was also demonstrated that the drug can be quantified in aqueous samples, such as river water. **Conclusions**
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