Physicochemical Properties and Volumetric Change of Silicone/Bioactive Glass and Calcium Silicate–based Endodontic Sealers

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Abstract

Introduction: This study evaluated setting time (ST), radiopacity, pH, flow, solubility, and volumetric change (VC) of a silicone, gutta-percha, and bioactive glass–based sealer, GuttaFlow Bioseal (GFB), and a calcium silicate–based sealer, TotalFill BC Sealer (TFBC), in comparison with AH Plus. Methods: ST and flow were evaluated in accordance with the ISO 6876 Standard. pH was evaluated after different time intervals (1, 3, 7, 14, 21, and 28 days). Radiopacity was evaluated by radiographic analysis in millimeters of aluminum. Solubility was evaluated by means of mass loss (%) after 7 and 30 days of immersion in distilled water. VC was evaluated by micro-computed tomography, by using cavities 3 mm deep and 1 mm in diameter in acrylic resin, filled with the materials. The materials were evaluated after setting and after 7 and 30 days of immersion in distilled water. The data were submitted to analysis of variance and Tukey statistical tests (P < .05). Results: TFBC demonstrated the highest pH and solubility. GFB had the shortest ST, and lowest radiopacity and flow values. VC was similar for the sealers in both time intervals. Conclusions: TFBC presented the highest pH and solubility, but showed similar VC to GFB and AH Plus. GFB showed proper physicochemical properties. Micro-computed tomography complements the physicochemical analysis of endodontic sealers. (J Endod 2017;43:2097–2101)

Key Words

Micro-computed tomography, physicochemical properties, root canal sealer

Significance

A silicone, gutta-percha, and bioactive glass–based sealer, GuttaFlow Bioseal, showed proper physicochemical properties, including volumetric change after evaluation by using ISO 6876 and micro-computed tomography (micro-CT) methods. Micro-CT complements the physicochemical analysis of endodontic sealers.

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Basic Research—Technology

The development of new endodontic sealers and new tests may enhance evaluation and knowledge about the behavior of these materials. The aim of this study was to evaluate the physicochemical properties of a silicone, gutta-percha, and bioactive glass–based sealer (GBB) and a calcium silicate–based sealer (TFBC) in comparison with AHP, by using conventional tests and volumetric change using micro-CT.

Materials and Methods

The endodontic sealers used in this study and their respective manufacturers are described in Table 1.

Physicochemical Properties: Conventional Methods

Setting Time. Plaster molds measuring 10 mm in diameter and 1 mm high were used to fabricate specimens of each material (n = 6). Plaster molds were immersed in water for 24 hours at 37°C, and then the cavities were filled with the material. Setting time (ST) was evaluated in accordance with the ISO 6876 (2). A Gilmore needle with mass of 100 ± 0.5 g and diameter of 2.0 ± 0.1 mm was used, supported on the sealer surface. The materials were kept in an oven at 37°C and 95% humidity. ST of the sealers was considered as the time when the marks of needle could not be observed on the sealer surface.

Radiopacity. Specimens (n = 5) measuring 10 mm in diameter by 1 mm thickness were made for each tested material. The radiopacity was evaluated according to Tanomaru-Filho et al (23). Each sample was positioned on 5 occusal radiographic films (Insight-Kodak Comp, Rochester, NY) and exposed, along with an aluminum step wedge with variable thickness (from 2 to 16 mm, in 2-mm increments). An X-ray unit (Instrumentarium Dental, Tuusula, Finland) operating at 60 kV, 7 mA, 0.32 pulses per second, and focus-film distance of 33 cm was used. The films were processed in a standard automatic processor (Dent-X 9000, Dent-X, Elmsford, NY). Radiographs were digitized, and the images were imported to the Image Tool 3.0 software (UTHSCSA, San Antonio, TX) to obtain the area of millimeter ruler. The images obtained were evaluated using the Image Tool 3.0 software (UTHSCSA, San Antonio, TX) to obtain the area of the radiographic images. Thus, the radiopacity of the evaluated sealers was estimated from the thickness of aluminum (in mm) by using a conversion equation. The values recorded for each material were averaged to obtain a single value in mm Al.

Solubility. Based on a previous study (24), circular plastic molds measuring 1.5 mm high and 7.75 mm in diameter were placed on a glass plate covered with cellophane film. These molds were filled with each of the materials by a single operator, who was previously trained and calibrated. The samples were kept in an oven at 37°C and relative humidity for 3 times the duration of their setting time. The test specimens were removed from the molds and weighed on a precision balance (HM-200; A & D Engineering, Inc., Bradford, MA). Then, they were placed in closed plastic flasks containing 7.5 mL of distilled and deionized water. The specimens were attached to the containers with nylon threads and kept in an oven at 37°C for 7 days. After this period, they were washed in distilled water, and placed in a dehumidifier. The mass was measured before and after the samples were immersed in distilled water, and every 24 hours thereafter, until the mass was stabilized. New samples were made and kept immersed in distilled water for 30 days. The loss of mass was expressed as a percentage of the original mass. In accordance with ISO and ANSI/ADA, the results must not exceed contraction of 1.0% or expansion of 0.1% pH.

pH polyethylene tubes (Embramed Ind. Com., São Paulo, SP, Brazil) measuring 10 mm length and 1.6 mm diameter were filled with freshly prepared samples of each material (n = 10). The tubes were immersed in plastic flasks containing 10 mL of deionized water. The flasks were closed and kept in an oven at 37°C. pH measurements were performed after 1, 3, 7, 14, 21, and 28 days. The solution’s pH was analyzed at each period using a previously calibrated digital pH meter (Digimed, São Paulo, Brazil). After each measurement (in triplicate), the mean pH of each group in each experimental period was calculated.

Flow. The flow test was conducted in accordance with ISO Standard 6876 (2). After manipulation of the sealer, 0.05 mL of the material was placed in the center of a glass plate using a graduated syringe (n = 10). At 180 ± 5 seconds after initiating the manipulation, another glass plate (20 g) was placed on the plate with the sealer, and a 100-gram weight was put on the top plate, and kept there for 10 minutes. After this period, the maximum and minimum diameters of the material on the glass plate were measured. When a difference of less than 1 mm between the diameters was observed, the mean value was recorded. A second evaluation was made by photographing the material on the plate alongside a millimeter ruler. The images obtained were evaluated using the Image Tool 3.0 software (UTHSCSA, San Antonio, TX) to obtain the area of flow of the material expressed in mm², according to Tanomaru-Filho et al (23).

Volumetric Change: Micro-Computed Tomography

Analysis

Volumetric change of the sealers was analyzed using micro-CT (Bruker-MicroCT, Kontich, Belgium). Transparent acrylic resin–based models were fabricated using metal molds with cavities measuring 3 mm deep and 1 mm in diameter (n = 6). The cavities were filled with each of the materials by a single operator, who was previously trained and calibrated. The samples were kept in an oven at 37°C and relative humidity for 3 times the duration of their ST. For TFBC setting, a piece of wet cloth was placed over the cavities.

<table>
<thead>
<tr>
<th>TABLE 1. Endodontic Sealers and Their Manufacturers</th>
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<tbody>
<tr>
<td>Endodontic sealer</td>
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</tr>
<tr>
<td>GuttaFlow Bioseal (GBB)</td>
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<tr>
<td>TotalFill BC Sealer (TFBC)</td>
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<td>AH Plus (AHP)</td>
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</table>
Then, the samples were scanned by micro-CT (Bruker-MicroCT). The samples were immersed in distilled water for 7 and 30 days and they were scanned again after these experimental time intervals. The scanning procedure was performed using 50 kV X-ray tube voltages and 500 μA anode current; aluminum filter of 0.5; isotropic voxel of 18 μm; and a 360° evolution cycle. The images were used for quantitative analysis of the samples, allowing the total volume of material to be calculated in mm³. A schematic figure of the volumetric change assessment is illustrated in Figure 1.

Reconstruction of the images was performed with NRecon software (V1.6.4.7; Bruker-MicroCT). The correction parameters for smoothing, beam hardening, and ring artifacts were defined for each material. The same parameters were used for the same material in different periods. The reconstructed images were superimposed on the different periods and saved in the coronal, sagittal, and transaxial planes by using the Data Viewer program (V1.5.2.4; Bruker-MicroCT). The images were analyzed with CTAn software (V1.11.8; Bruker-MicroCT). The volume filled by the sealers was calculated at each time interval. A 3-dimensional model of the filled cavities was obtained by using the CTVol software (V2.0; Bruker-MicroCT) (Fig. 2).

Statistical Analysis

Preliminary data analysis was performed with the Shapiro-Wilk test. Statistical analysis was performed with parametric tests. The analysis of variance and Tukey comparison tests were used. The level of significance was set at $P < .05$.

Results

The results are represented in Tables 2 and 3. GFB presented shorter ST (30 minutes) and TFBC the highest value ($P < .05$) (Table 2). GFB presented the lowest radiopacity value (3.9 mm Al) in comparison with the other sealers ($P < .05$), and AHP, the highest value (9.42 mm Al).

The solubility value was higher for TFBC when compared with those of the other materials ($P < .05$) and AHP, the lowest value (Table 2). The pH was higher for TFBC, followed by GFB, in the whole experimental period (Table 3). GFB presented the lowest flow values ($P < .05$) in comparison with the other sealers. No statistically significant difference between the root canal sealers in both time intervals was observed for volumetric change test ($P > .05$).

Discussion

Standardized tests for evaluating the physicochemical properties of endodontic sealers have been recommended by ISO/ADA (1, 2). Carvalho-Junior et al (24) proposed specimens with smaller dimensions for the solubility test, without affecting the accuracy of the methodology. The solubility of root canal sealers is evaluated by the difference in the material mass before and after immersion in distilled water.
TABLE 2. Setting Time, Radiopacity, Solubility, Flow, and Volumetric Change Values (Mean and Standard Deviation)

<table>
<thead>
<tr>
<th>Test/Materials</th>
<th>AH Plus</th>
<th>Total Fill BC Sealer</th>
<th>GuttaFlow Bioseal</th>
</tr>
</thead>
<tbody>
<tr>
<td>Setting time, min</td>
<td>384 (±0.09)b</td>
<td>581.5 (±27.18)a</td>
<td>30.67 (±0.82)c</td>
</tr>
<tr>
<td>Radiopacity, mm Al</td>
<td>9.42 (±0.39)a</td>
<td>6.15 (±0.39)b</td>
<td>3.94 (±0.21)c</td>
</tr>
<tr>
<td>Solubility 7 days, % mass loss</td>
<td>0.041 (±0.05)c</td>
<td>7.444 (±0.86)a</td>
<td>2.938 (±0.45)b</td>
</tr>
<tr>
<td>Solubility 30 d, % mass loss</td>
<td>0.406 (±0.27)c</td>
<td>13.49 (±0.71)a</td>
<td>4.812 (±1.22)b</td>
</tr>
<tr>
<td>Flow, mm</td>
<td>21.41 (±1.14)b</td>
<td>24.83 (±0.79)a</td>
<td>16.88 (±0.40)c</td>
</tr>
<tr>
<td>Flow, mm²</td>
<td>407.2 (±114.2)b</td>
<td>535.4 (±52.75)a</td>
<td>240.8 (±11.52)c</td>
</tr>
<tr>
<td>Volumetric change 7 d, %</td>
<td>0.50 (±0.46)a</td>
<td>0.62 (±0.32)a</td>
<td>0.14 (±0.16)a</td>
</tr>
<tr>
<td>Volumetric change 30 d, %</td>
<td>-0.19 (±0.93)c</td>
<td>-1.07 (±0.51)a</td>
<td>-0.68 (±0.94)a</td>
</tr>
</tbody>
</table>

mm Al, aluminum millimeter; % mass loss, percentage of mass loss.
abdDifferent letters in the same row showed statistically significant difference.

TABLE 3. pH Values (Mean and Standard Deviation) at the Different Experimental Periods

<table>
<thead>
<tr>
<th>Experimental periods</th>
<th>AH Plus</th>
<th>Total Fill BC</th>
<th>GuttaFlow Bioseal</th>
<th>Control</th>
</tr>
</thead>
<tbody>
<tr>
<td>1 day</td>
<td>6.583 (±0.16)c</td>
<td>10.37 (±0.20)a</td>
<td>8.203 (±0.46)b</td>
<td>6.480 (±0.27)c</td>
</tr>
<tr>
<td>3 days</td>
<td>6.589 (±0.22)c</td>
<td>10.61 (±0.16)a</td>
<td>8.202 (±0.49)b</td>
<td>6.422 (±0.23)c</td>
</tr>
<tr>
<td>7 days</td>
<td>5.957 (±0.22)a</td>
<td>10.29 (±0.21)a</td>
<td>8.512 (±0.25)b</td>
<td>6.248 (±0.10)c</td>
</tr>
<tr>
<td>14 days</td>
<td>6.428 (±0.43)a</td>
<td>10.53 (±0.14)a</td>
<td>7.573 (±0.14)b</td>
<td>6.200 (±0.12)c</td>
</tr>
<tr>
<td>21 days</td>
<td>6.040 (±0.20)a</td>
<td>9.500 (±0.93)a</td>
<td>7.388 (±0.14)b</td>
<td>6.368 (±0.23)c</td>
</tr>
<tr>
<td>28 days</td>
<td>5.672 (±0.25)c</td>
<td>9.213 (±0.86)a</td>
<td>7.238 (±0.29)b</td>
<td>6.320 (±0.22)c</td>
</tr>
</tbody>
</table>

Control, distilled water.
abdDifferent letters in the same row showed statistically significant difference.

water. This test has limitations, because materials may present degradation during storage or absorb water (22). Therefore, the use of micro-CT may complement conventional tests, providing additional data about volumetric changes in materials (19–21).

According to the present study, GFB demonstrated shorter ST than TFBC and AHP sealers, in agreement with Gandolfi et al (15), who suggested that the presence of calcium silicate in GFB reduced its ST when compared with GuttaFlow. TFBC sealer showed the longest ST.

The radiopacity of all the sealers showed values in accordance with ISO. AHP was the most radiopaque sealer, followed by TFBC and GFB. The differences in radiopacity of the root canal sealers evaluated may be related to the presence of radiopaque agents in each material (25). These agents have the following decreasing order of radiopacity: bismuth oxide, zirconium oxide, calcium tungstate, barium sulphate, and zinc oxide (26). The quantity and proportion of each radiopaque agent may interfere in the radiopacity of the cements. Therefore, the presence of calcium tungstate in addition to the zirconium oxide in the AHP cement provided the material with higher radiopacity (25), whereas TFBC and GFB presented only zirconium oxide in their composition.

Calcium silicate cements provide an alkaline pH, as a result of calcium ion release (15). TFBC demonstrated the highest pH values, as observed by Zhou et al (10) for the EndoSequence BC Sealer. GFB was the sealer with the second highest pH value, which may have occurred as a result of its capacity for forming hydroxyapatite, due to the presence of bioactive ceramic glass, in spite of its low calcium release values (15). The alkalinity demonstrated may contribute to the osteogenic potential, biocompatibility, and antibacterial capacity of this material (10). Furthermore, it has been suggested that the mechanism of mineralized tissue repair depends on the pH and capacity for releasing Ca²⁺ of the material (27).

Higher solubility was observed for the TFBC that showed high calcium ion (15) and hydroxyl release values. The lowest values were observed for AHP, which may be related to the crossed links in its resin polymers (28) that promoted low solubility (29).

Volumetric change of the material after immersion in distilled water may be observed by using micro-CT. Cavenago et al (19) evaluated MTA with different powder-water ratios and associated the loss of volume with the solubility of the material. The solubility of materials cannot be related exclusively to the volumetric behavior, particularly for calcium silicate–based cements that may absorb water (21). Therefore, Torres et al (21) evaluated the volumetric change in reparative cements after setting and immersion in distilled water for time intervals of 7 and 30 days. Silva et al (20) used the volumetric change test to observe the behavior of root canal sealers after immersion in PBS solution for 7 days.

The results of the present study demonstrated similar volumetric change values for all the sealers studied, differently from that which occurred in the conventional solubility test, when TFBC was the material that showed the highest loss of mass values and AHP, the lowest. Therefore, we must consider that volumetric changes do not depend on the solubility of cements only, but also on dimensional changes such as contraction or expansion (20, 21). Gandolfi et al (15) observed low solubility and high water sorption for GFB, suggesting that the material may exhibit expansion and mass loss. So, the solubility of this sealer after 7 days could be compensated by the fluid absorption (3), resulting a volume increase. After 30 days, we observed volumetric reduction probably because the solubility was higher than water absorption. Similarly, the higher solubility of TFBC in the conventional solubility test may have been compensated by the absorption of fluids that occurred in calcium silicate–based cements, resulting in their volumetric stability (20). The volumetric change test must be considered an additional test to the solubility test and present correlation with its clinical performance.

Previous studies have observed that TFBC showed high bond strength values in the push-out test (12, 13), which suggested that the calcium silicate–based sealers provide good adaptation to dentin (14). The good penetrability of these materials may be explained as being due to the reduced size of its cement particles (30) and probably due to the adequate flow values that were observed in the present study.

In conclusion, TFBC sealer presented the highest ST, pH, solubility, and flow values, in addition to similar volumetric change to that of the other sealers studied. GFB showed adequate physicochemical properties. Micro-CT can complement conventional tests, allowing better knowledge of the behavior of materials, and improving its clinical application.
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The authors deny any conflicts of interest related to this study.

References


