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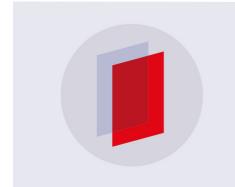
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Nanotechnology 29 (2018) 365701 (10pp)

https://doi.org/10.1088/1361-6528/aacc21

Synthesis, characterization and applications of maghemite beads functionalized with rabbit antibodies

A F R Rodriguez^{1,6}, C O Rocha⁵, R D Piazza⁵, C C dos Santos⁵, M A Morales², F S E D V Faria¹, M Zubair Iqbal³, L Barbosa⁴, Y O Chaves⁴, L A Mariuba⁴, M Jafelicci Jr⁵ and R F C Marques⁵

E-mail: anselmorodriguez73@gmail.com

Received 23 January 2018, revised 4 June 2018 Accepted for publication 12 June 2018 Published 28 June 2018



Abstract

Magnetic nanoparticles (NPs) have attracted great attention owing to their applications in the biomedical field. In the present work, maghemite (γFe_2O_3) NPs of 6.5 nm were prepared using a sonochemical method and used to prepare magnetic beads through silanization with 3-aminopropyltrimethoxysilane (APTS). Subsequently, amino groups in the resulting APTS- γFe_2O_3 beads were converted to carboxylic acid (CARB- γFe_2O_3) through the succinic anhydride reaction, as confirmed by transmission electron microscopy (TEM), Fourier transform infrared spectroscopy and dynamic light scattering (DLS) measurements. The size of these beads was measured as 12 nm and their hydrodynamic diameter as 490 nm, using TEM analysis and DLS, respectively. The CARB- γFe_2O_3 beads were further functionalized by immobilizing rabbit antibodies on their surfaces; the immobilization was confirmed by flow cytometry and ionic strength. The samples were further characterized by Mössbauer spectroscopy and DC magnetization measurements. Studies on magnetic relaxivities showed that magnetic beads present great potential for application in MR imaging.

Keywords: magnetic nanobeads, flow cytometry, MRI, mössbauer spectroscopy, XRD, rabbit antibody

(Some figures may appear in colour only in the online journal)

1. Introduction

During the last few decades, researchers have been developing methods for the immobilization of proteins and enzymes on magnetic nanoparticles (NPs) [1], useful for magnetic resonance imaging (MRI) [2]. Various methods have been employed to synthesize iron oxide magnetic NPs, among the most common being co-precipitation [3], sol-gel [4], solid state [5], sonochemical [6], microwave assisted [7] and thermal decomposition [8]. These solution based methods allow the production of NPs with controllable size, morphology and crystallinity, and variable surface chemistry. Their biocompatibility and appropriate functionalization are key conditions for their use in biomedicine [9]. Magnetic iron oxide NPs show superparamagnetic behavior, very low coercivity and high magnetic moment per gram of sample. To

¹ Federal University of Acre, Laboratory of Nanobiotechnology, Rio Branco, 69920-900, AC, Brazil

² Federal University of Rio Grande do Norte, Department of Theoretical and Experimental Physics, Natal, 59078-970, RN, Brazil

³ Division of Functional Materials and Nano-Devices, Ningbo Institute of Materials Technology & Engineering, Chinese Academy of Sciences, People's Republic of China

⁴ Instituto Leonidas e Maria Deane, Fundação Oswaldo Cruz, Adrianópolis, 69057-070, AM, Brazil

⁵ São Paulo State University—UNESP, Laboratory of Magnetic Materials and Colloids, Institute of Chemistry, Caixa postal 355, Araraquara 14800-900, SP, Brazil

⁶ Author to whom any correspondence should be addressed.

provide stability in water, iron oxide NPs are usually capped with a variety of functional groups such as amino (-NH2) and carboxylic groups (-COOH). Magnetic beads are small particles consisting of a non-magnetic matrix—e.g. silica or polystyrene—with embedded ferromagnetic NPs [10]. This allows the manipulation of beads through magnetic forces, but avoids agglomeration of the beads since no permanent magnetic moment remains after removing an external magnetic field.

A wide selection of silica-coated magnetic NPs can be used as substrates for the attachment, through polar interactions, of a broad range of biomolecules. However, proteins do not normally bind effectively to silica beads; thus, a simple treatment to have more reactive surface groups, such as carboxylic groups (-COOH) [11] will greatly enhance protein binding.

The large surface-to-volume ratio of magnetic beads provides a further use for chemical bonding of target macromolecules [12]. Magnetic beads are well established for manipulation of biomolecules, such as proteins, cells, or bacteria [13], and can be applied in magnetic bioseparations [14]. Magnetic beads may also serve as contrast enhancing agents for MRI, for releasing heat upon absorption of radio frequencies, or they may be used for magnetic drug targeting [15, 16].

In this work, we will summarize a chemical route for the synthesis of magnetic beads using APTS and maghemite. Modification of the bead's surface was performed by succinic anhydride reaction. We have used rabbit antibodies to prove the ability of magnetic beads to couple proteins on their surface. The physical and chemical properties of magnetic beads were studied using Fourier transform IR spectroscopy (FTIR), zeta potential, transmission electron microscopy (TEM), x-ray diffraction analysis (XRD), dynamic light scattering (DLS), DC magnetization, Mössbauer spectroscopy and flow cytometry. Finally, we will apply the beads in various aqueous concentrations for MRI and in high-resolution molecular imaging.

2. Experimental

2.1. Materials

All chemicals were used as received from suppliers:

Iron (II) chloride tetrahydrate (97%), succinic anhydride (99.0%) and 3-aminopropyltrimethoxysilane (APTS) (98.0%) were purchased from Sigma-Aldrich Brazil. Dimethylformamide (DMF, 99.9%) was acquired from Panreac. Sodium hydroxide (NaOH, 97%) and ammonium hydroxide (NH₄OH, 30% (v/v)) were purchased from Synth. Iron (III) chloride hexahydrate and sodium chloride (99.0%) were purchased from Mallinckrodt Chemicals.

2.2. Synthesis of magnetic NPs (γ Fe₂O₃) and beads with amine groups (APTS- γ Fe₂O₃)

Magnetite was synthesized by sonoprecipitation method [17]. The NPs were obtained by dissolving 1.019 g of $FeCl_2 \cdot 4H_2O$ and 2.773 g of $FeCl_3 \cdot 6H_2O$ (in a molar ratio1:2) in 80 ml of

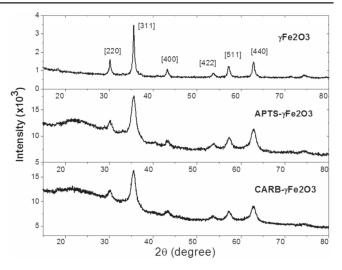


Figure 1. Diffraction patterns of bare iron oxide γFe_2O_3 , APTS- γFe_2O_3 and CARB- γFe_2O_3 beads. Numbers are the Miller indices.

distilled water. An aqueous solution at $80\,^{\circ}\text{C}$ was prepared with sodium hydroxide and $1.0\,\text{ml}$ aliquots of $H_2\text{O}$ added until the solution reached pH 12. Then $1.6\,\text{ml}$ of the iron solution was added to the above alkaline solution. This solution was agitated with an ultrasonic tip probe for one hour, with 3 s of pulse on and 3 s of pulse off. Transformation of magnetite to maghemite occurred after exposing the aqueous suspension of NPs to air at room temperature for one week.

To prepare magnetic beads, we added 200 μl of APTS to the above maghemite suspension. The as-produced beads were labeled as APTS- γFe_2O_3 .

2.3. Synthesis of beads with carboxylic groups (CARB- γFe_2O_3)

In a second step, 200 mg of APTS- γ Fe₂O₃ beads was dispersed in 30 ml of dimethylformamide (DMF). A solution of 0.3 g of succinic anhydride and 20 ml of DMF was prepared. These solutions were mixed and placed in a distillation flask with bubbling argon at room temperature and for 8 h [18].

2.4. Functionalization of magnetic beads with rabbit antibodies

The functionalization of magnetic beads with rabbit antibodies was done by using the methodology reported by Greg [19]—briefly, 20 mg of maghemite beads were washed three times with phosphate buffer (0.01 M) and re-suspended in 1 ml of ultrapure water. Then, 1 ml of rabbit antibody at various concentrations (10, 8, 5, 2.5, 2, 1 and 0.5 μ g ml⁻¹), 400 μ l (0.54 mg ml⁻¹) EDAC (1-ethyl-3-(3-dimethylamino-propyl)carbodiimide, hydrochloride) and 5 mM NHS (N-hydroxysuccinimide) were added to the magnetite dispersion. The beads were washed again, and the blocking buffer (1 M glycine at pH 8.0) was added and mixed for 1 h. Then, fluorescent secondary antibody (Anti-rabbit Alexa 488) was added at the dilution of 1/200, incubated for 30 min, and washed twice with PBS. Finally, the magnetic beads were measured by flow cytometry (FACS Canto II).

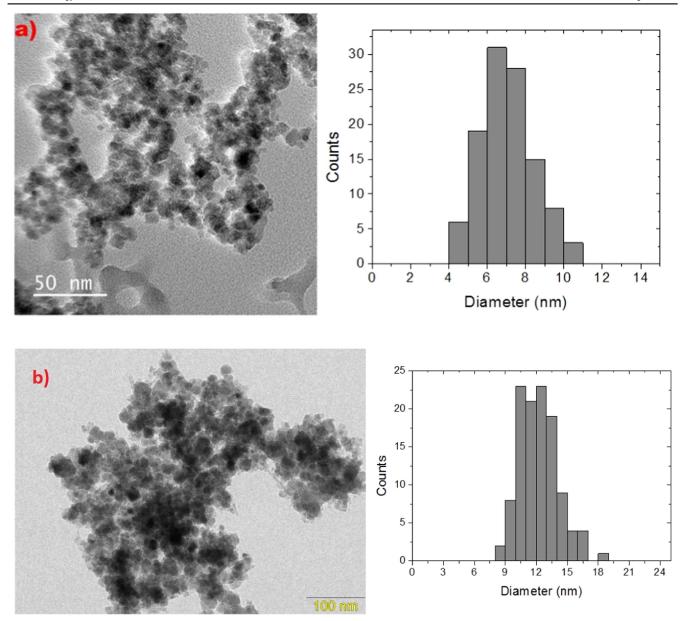


Figure 2. (a) TEM micrograph of bare γFe_2O_3 NPs, and their size distribution. (b) TEM micrograph of APTS- γFe_2O_3 beads, and their size distribution.

2.5. XRD measurements

Structural characterization of samples was carried out with XRD using a MiniFlexII Rigaku diffractometer equipped with a CuK α radiation source. XRD data were collected in the 2θ range between 10° and 85° with a scan rate of $5^{\circ}/\text{min}$ and steps of 0.02° .

2.6. TEM

A TEM micrograph was obtained on a Philips CM120 microscope. The beads were dispersed in isopropanol and one drop of the dispersion was deposited on a carbon covered copper grid.

2.7. Infrared spectroscopy (FTIR)

FTIR spectra were recorded in the reflectance mode on a Perkin—Elmer Frontier spectrometer to identify the composition of the NPs and the lipase content. The samples were milled, dispersed in KBr and pressed into pellets. Spectra were recorded in the range of 4000–400 cm⁻¹ with a nominal resolution of 4.0 cm⁻¹ and through 64 scans.

2.8. Zeta potential and DLS measurements

Zeta potential and the particles' hydrodynamic size were measured using a Zetasizer Nanoseries NanoZS, from Malvern Instruments. For Zeta potential measurements, the samples were previously suspended in NaCl $1\,\text{mmol}\,\text{L}^{-1}$

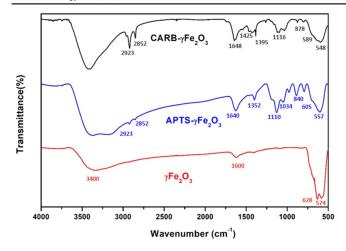


Figure 3. Infrared spectroscopy of γFe_2O_3 , APTS- γFe_2O_3 and CARB- γFe_2O_3 samples.

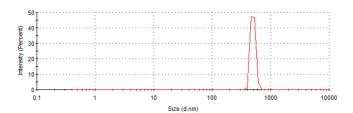


Figure 4. DLS of APTS- γ Fe₂O₃ NPs dispersed in water.

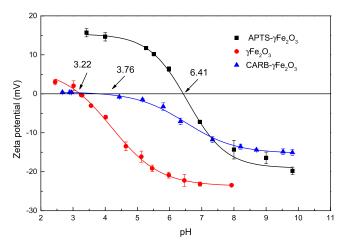


Figure 5. pH dependence of Zeta potential of γFe_2O_3 , APTS- γFe_2O_3 and CARB- γFe_2O_3 samples.

solution. The Zeta potential was evaluated in the pH range of 2-10 and the samples were titrated with NaOH and HCL 0.1 mol L^{-1} solution.

2.9. Flow cytometry

The samples were analyzed by FSC (Forware Scatter) size, SSC (Side Scatter) granularity and fluorescence in a flow cytometer (FACS Canto®II), and the results were analyzed using FlowJo® software version 9.3.2 of the Tree Star © with the flow cytometry platform at Fiocruz-ILMD.

2.10. Mössbauer spectroscopy

⁵⁷Fe Mossbauer spectra were recorded in the transmission mode at 300 and 12 K by using a spectrometer from SEECo equipped with a helium closed cycle cryostat from Janis; the gamma ray source had an activity of 25 μ Ci. The spectra were fitted by using Normos90 software; the reported isomer shifts are related to α-Fe metal at room temperature.

2.11. Magnetic characterization

DC magnetization measurements were made in a physical properties measurement system, (PPMS-Dynacool from Quantum Design) equipped with a vibrating sample magnetometer (VSM). The magnetization as a function of temperature was determined in the zero field cooled (Mzfc) and field cooled (Mfc) modes under a magnetic field of 70 Oe; both measurements were made in the warming mode.

2.12. MRI

The transverse (T_2) and longitudinal (T_1) relaxation times and relaxivities (r_2, r_1) of as-prepared NPs were performed on a 0.55 T MRI instrument (Shanghai Niumai Corporation Ration NM120-Analyst). Dilutions of iron oxide NPs samples in water with various concentrations (0.08, 0.18, 0.36, 0.72 and 1.43 mM) were used for transverse and longitudinal relaxation times and T_2 imaging with additional concentrations (2.84 and 5.68 mM) as compared to water. Relaxation times T_2 and T_1 measurements were performed using TE (echo time) = 20 ms and TR (repetition time) = 4000 ms. T_2 -weighted MR images were performed on running a SE (spin-echo) sequence with TR = 1600 ms and TE = 20 ms.

3. Results and discussion

3.1. Structural characterization

3.1.1. XRD. The patterns of bare maghemite particles and beads are shown in figure 1. The diffractograms show peaks relative to the inverse spinel structure due to maghemite, no second phase like hematite or ferrihydrite was found. By using the Scherrer equation and the full width half maximum of the peak [311], [220], [511] and [440] we have determined the γFe_2O_3 particle size of (6.9 ± 0.9) nm, the samples APTS- γFe_2O_3 and CARB- γFe_2O_3 presented similar crystallite sizes to the bare γFe_2O_3 NPs, revealing that the procedure of coating with succinic anhydride and 3-aminopropyltrimethoxysilane do not affect the magnetic core. In the APTS- γFe_2O_3 and CARB- γFe_2O_3 patterns, the broad peak at about 22° is related to the amorphous SiO2. The diffraction peaks in figure 1 are consistent with the standard structure of maghemite (JCPDS card No. 39-1346).

3.1.2. TEM analyses. A TEM image of bare γFe_2O_3 NPs is presented in figure 2(a) along with their size distribution; the NPs have a spherical morphology and are not aggregated. The size distribution has a mean diameter of 6.5 nm. This result is

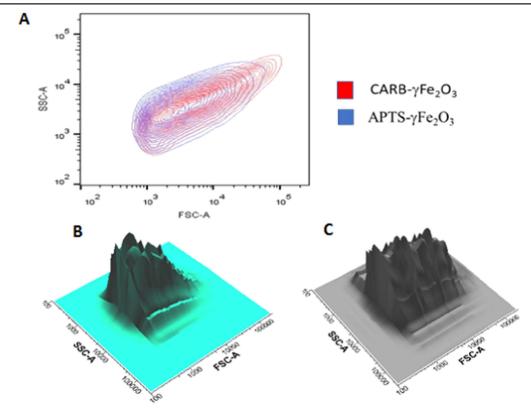


Figure 6. Overlap of APTS- γ Fe₂O₃ and CARB- γ Fe₂O₃ beads by FSC size and complexity SSC (A), surface chart of the correlation between FSC, SSC and the amount of NPs demonstrated by the APTS- γ Fe₂O₃ beads (B) and CARB- γ Fe₂O₃ beads (C).

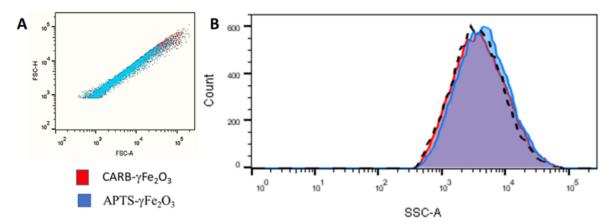


Figure 7. Evaluation of the uniformity of the samples correlating the size of the FSC-A area by the FSC-H height.

in close agreement with the crystallite size obtained in the XRD analysis.

A TEM image of APTS- γFe_2O_3 beads is presented in figure 2(b) along with their size distribution; the beads have a rounded morphology and form small agglomerates. The size distribution of the sample has a mean diameter of 12 nm. This result confirms the SiO₂ coating of the γFe_2O_3 NPs.

3.2. Vibrational characterization of magnetic beads

3.2.1. Infrared spectroscopy. The FTIR spectrum presented in figure 3 shows bands at 628 and 574 cm⁻¹ which are assigned to the Fe–O stretching vibration in γ Fe₂O₃, these bands appear

slightly shifted in the spectra of the APTS- γFe_2O_3 and CARB- γFe_2O_3 samples. The bands at 3400 and 1600 cm⁻¹ correspond to the O–H stretching and bending vibrations of adsorbed water, respectively [20]. The spectrum of the APTS- γFe_2O_3 sample has absorption bands at $1034~\rm cm^{-1}$ and $1110~\rm cm^{-1}$ which correspond to Si–O stretchings, confirming the silanization reaction. The amine group shows N–H out-of-plane bending at $870~\rm cm^{-1}$ and C–N stretchings at $1352~\rm cm^{-1}$. The asymmetric and symmetric absorption bands at $1648~\rm and$ $1425~\rm cm^{-1}$ correspond to carboxylate stretching vibrations, and confirm the functionalization with succinic anhydride. The bands located in between $1425-1380~\rm cm^{-1}$ are a combination of C–O stretchings and O–H deformation vibration. The band at

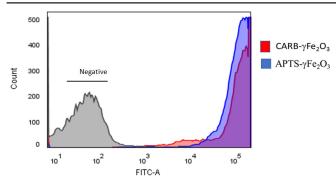


Figure 8. Overlays of the histograms showing the fluorescence of the secondary Alexa 488 Anti-Rabbit in the APTS- γ Fe₂O₃ and CARB- γ Fe₂O₃ beads conjugated in 10 μ g concentrations of primary rabbit.

1264 cm $^{-1}$ indicates the presence of carboxylic acid dimer [20]. Furthermore, the signals at 2923 cm $^{-1}$ and 2852 cm $^{-1}$, correspond to asymmetric and symmetric C–H vibrations, these bands are also observed in CARB- γ Fe₂O₃ and APTS- γ Fe₂O₃ samples.

3.2.2. DLS and zeta potential. Figure 4 shows the DLS measurement of APTS- γ Fe₂O₃ particles in water. It shows beads with hydrodynamic mean diameter of 490 nm. Comparison of bead size from DLS and TEM techniques reveal aggregation of this sample.

In addition, the magnetic beads were evaluated by Zeta potential measurements. The isoelectric point (IEP) corresponds to the regime where the net charge on the NPs is zero. The zeta potentials as a function of pH curves are shown in figure 5. The IEP for γFe_2O_3 NPs is located at pH = 3.22. It can be seen that the polycondensation with APTS shifted the IEP to 6.41, which corresponds to the APTS pKa value. Therefore, the APTS- γFe_2O_3 beads have a positive electrical potential at low pH (<6.41) and negative potential at high pH [21, 22]. Similar behavior is observed after functionalization of APTS- γFe_2O_3 beads with succinic anhydride. The pKa value of succinic acid is 4.2, while the IEP for CARB- γFe_2O_3 is at 3.76; this result confirms the functionalization of APTS- γFe_2O_3 with carboxylic groups.

3.3. Morphometric analysis of beads (size and complexity)

The morphometric characteristics of the NPs were analyzed by flow cytometry via the fluorescence detector parameters that measure the degree of direct scattering (FSC, *Y*-axis), and the degree of lateral dispersion or complexity—lateral dispersion (SSC, *X*-axis), and plotted on a logarithmic scale (figure 6(A)). The results show that the APTS- γ Fe₂O₃ beads were smaller in size than the CARB- γ Fe₂O₃ beads observed in 3D-size plots by complexity (figures 6(B), (C)).

3.3.1. Morphometric analysis of beads (uniformity). Although the initial morphometric characteristics showed that the particles had different sizes, it was verified that there was aggregation between the particles during the treatment; the singlet was analyzed by checking the particle uniformity in the parameters of lateral dispersion intensity (SSC-A) and uniformity (FSC-A) and (FSC-H). The results show that there is no difference between mean lateral dispersion intensity in both particle types compared to the untreated control (figure 7(B)) and that the particles follow a uniformity pattern (figure 7(A)) of 98.7% for APTS- γ Fe₂O₃ and 97.4% for CARB- γ Fe₂O₃.

Thus, we have performed several experiments to characterize the morphometric parameters of the beads essential to applications in biotechnology; the purity analysis can facilitate the identification of beads by flow cytometry.

3.3.2. Evaluation of fluorescence coupling capacity in beads. The uniformity of the samples correlating the size of the FSC-A area by the FSC-H height (see figure 8) was also evaluated, showing that both samples have approximately uniform sizes comprising 92.2% and 92.9% within the analysis range, respectively.

Two subpopulations of coupled NPs were analyzed, in order to determine the percentage of fluorescence coupling according to the types of pretreatment; these results are presented in table 1.

The percentage of coupling is calculated by the initial analysis of the percentage of events within the gate determined by size and complexity (figure 6); after determining the area of analysis of the beads, the percentage of fluorescence is determined in relation to the beads without coupling or cut off. The fluorescence above the cut line determines the percentage of fluorescence (figure 8) calculated through the Flowjo program or by multiplying the fluorescence gate (fluorescence) mean by the gate (count) of size and complexity.

In the fluorescence analysis, the histograms show that both samples have about 95% coupling; this is confirmed in figure 8 by the overlapping histogram graph, that shows two populations of magnetic NPs: low coupling and high coupling (see table 1). ATPS- γ Fe₂O₃ magnetic beads exhibited larger populations with high coupling percentage (93.3%) when compared to CARB- γ Fe₂O₃ magnetic beads (85%) at either of the 10 μ g or 0.5 μ g of rabbit antibody concentrations shown in table 1. However, no significant variation of fluorescence between dilutions of the antibody in the coupling was observed, indicating that a test with smaller antibody values would be required in order to determine the best concentration for coupling and the limiting dilution.

3.4. Magnetic studies

Figure 9 shows the magnetization as a function of magnetic field of CARB- γ Fe₂O₃ and ATPS- γ Fe₂O₃ beads. At 300 K, the CARB- γ Fe₂O₃ and ATPS- γ Fe₂O₃ samples showed saturation magnetizations of 27.4 emu g⁻¹ and 26.4 emu g⁻¹, respectively. At 5 K, their saturation magnetizations were of 35.5 emu g⁻¹ and 33.9 emu g⁻¹ for CARB- γ Fe₂O₃ and ATPS- γ Fe₂O₃ beads, respectively. The low saturation magnetization is due to the SiO₂ contribution to the sample mass—as shown in figure 2, there is a thick layer of SiO₂ on the surfaces of - γ Fe₂O₃ NPs—and to the

Table 1. Percentage of APTS- γ Fe₂O₃ and CARB- γ Fe₂O₃ beads coupled with antibodies separated into high coupling and low coupling.

Sample	High %		Low %	
	$\overline{\text{APTS-}\gamma\text{Fe}_2\text{O}_3}$	CARB-γFe ₂ O ₃	$\overline{\text{APTS-}\gamma\text{Fe}_2\text{O}_3}$	CARB-γFe ₂ O ₃
CN	0	0.052	0.37	2.57
$10 \mu \mathrm{g}$	95.2	88.1	4.62	10.4
$8 \mu g$	88.9	76.2	11	2.7
$5 \mu g$	93.1	87	6.8	10.6
$2.5 \mu\mathrm{g}$	95.9	82.4	3.92	15.9
$2 \mu g$	90.9	89	8.94	9.32
$1~\mu \mathrm{g}$	96.6	81.1	3.29	14.2
$0.5~\mu\mathrm{g}$	94.8	91	4.89	7.86
Mean	93.3	85	6.21	12.7
SD	2.83	5.24	2.85	4.49

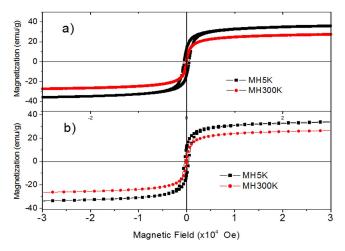


Figure 9. M—H curves at 5 K and 300 K for (a) Carboxylic acid (CARB- γ Fe₂O₃) beads and (b) ATPS (ATPS- γ Fe₂O₃) beads.

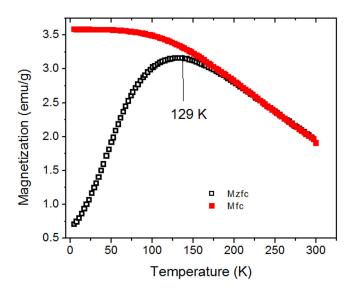


Figure 10. Mzfc and Mfc measurement under a field of 70 Oe for ATPS- γ Fe₂O₃ beads.

reduced $\gamma \text{Fe}_2\text{O}_3$ particle size, which enhances the total surface of the sample; in this case, the outer Fe layers have broken bonds and their Fe moments may experience a canting effect and therefore show a lower saturation magnetization [23].

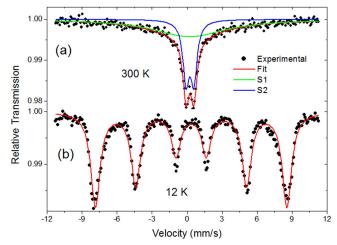


Figure 11. Mössbauer spectroscopy measurements performed at (a) 300 K and (b) 12 K for CARB- γ Fe₂O₃ beads.

At room temperature the coercivity field for CARB- γ Fe₂O₃ and ATPS- γ Fe₂O₃ samples were smaller than 50 Oe. Although the NPs are below the critical size to be superparamagnetic at room temperature, the low coercivity field suggest that there is some agglomeration of NPs and there are dipolar interactions between them.

Figure 10 shows the Mzfc and Mfc measurements performed for the ATPS- γ Fe₂O₃ sample. The cusp observed at $T_B^{VSM}=129~\rm K$ indicates the thermal blocking temperature for the ATPS- γ Fe₂O₃ NPs, this temperature may be larger than expected for a system of NPs without interaction [24]. The magnetic dipolar interaction between NPs can be studied through long-range dipolar forces in terms of the interacting superparamagnetic model and the Vogel–Fulcher law [24]. Since the CARB- γ Fe₂O₃ sample was obtained by functionalization of the ATPS- γ Fe₂O₃ sample with succinic acid, it is reasonable to conclude that both samples should have similar blocking temperatures.

The 57 Fe Mössbauer spectra for the CARB- γ Fe₂O₃ sample is presented in figure 11. The spectrum recorded at room temperature, figure 11(a), is analyzed by taking into account a broad spectrum (S1) due to slow relaxing Fe magnetic moments, and a doublet (S2) related to fast relaxing Fe magnetic moments. The doublet has isomer shift and

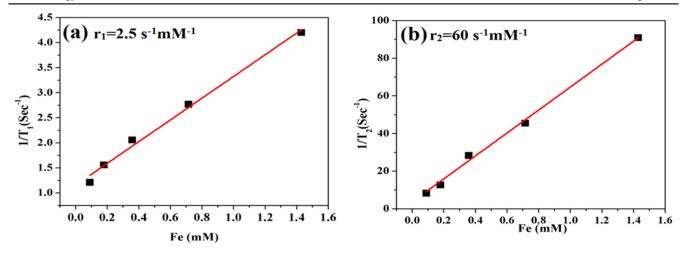


Figure 12. MRI relaxation time of the as-prepared beads CARB- γ Fe₂O₃ at various concentrations of Fe (0.08, 0.18, 0.36, 0.72 and 1.43 mM).

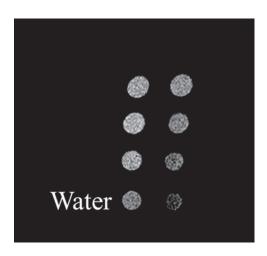


Figure 13. T2 MR imaging of pure water and CARB- γ Fe₂O₃ beads at various concentrations of Fe (0.08, 0.18, 0.36, 0.72, 1.43, 2.14 and 2.85 mM).

quadrupole splitting in agreement with Fe³⁺. The relative absorption spectral areas (RAA) are of 63% and 37% for the S1 and S2 Fe components. Since RAA(S1)/RAA(S2) > 1, we can conclude that this sample is thermally blocked at 300 K. This result does not contradict the M–H analyses because the Mössbauer spectroscopy measuring time (of $\sim 10^{-7}$ s) is smaller than the magnetometry measuring time (~ 10 s); this fact will lead to a higher Mössbauer blocking temperature.

⁵⁷Fe Mössbauer spectroscopy is an element-specific technique which provides local information on the spin relaxation and charge of iron ions, and allows an easy identification of iron oxides through their hyperfine magnetic field, isomer shift and quadrupole splitting [25].

The measurement recorded at 12 K is shown in figure 11(b). This spectrum exhibits a single sextet with hyperfine magnetic field of 51 T and isomer shift of 0.38 mm s⁻¹; both parameters are in close agreement with the formation of maghemite [25]. No other second phase containing Fe was observed.

3.5. Magnetic resonance studies

Interest in the use of nanometric particles has increased over recent years, and has been applied in several studies. Many studies have sought to characterize and investigate applications, even proposing the use of the tool as a diagnostic test material due to its easy applicability. Flow cytometry has been used as a tool to evaluate the morphometric characteristics [26] and coupling capacity [27] of these compounds, as well as the interaction which these NPs can have with human cells, increasing the applicability of these compounds in the field of immunology [27-30]. In our study, beads prepared with APTS- γ Fe₂O₃ and CARB- γ Fe₂O₃ showed similar morphologies (figure 6) as well as sample uniformity (figure 7). The ability to investigate these morphological parameters and the coupling capacity of these NPs analyzed by flow cytometry may be fundamental for the development of a future tool for applications in nanobiotechnology [31–33].

In order to examine the features of as-synthesized beads CARB- γ Fe₂O₃ as an MR contrast agent, magnetic relaxation times and T_2 magnetic resonance images were measured on 0.55 T scanner.

The longitudinal and transverse relaxation times (r_2, r_1) of CARB- γ Fe₂O₃ beads are shown in figures 12(a), (b). The r_1 value is 2.5 s⁻¹mM⁻¹ and the r_2 value 60 s⁻¹mM⁻¹, giving an r_2/r_1 ratio of 24— demonstrating that the fabricated beads are an efficient T_2 weighted contrast agent.

Furthermore, to prove the relation time in the favor of T_2 contrast agent, MR imaging was acquired. Figure 13 shows the T_2 -weighted MRI of beads and water. It is clearly seen that the MRI signals of NPs becomes brighter at initial low concentration because of the size of the NPs and then become darkened at high concentration as compared to the MRI image of pure water. The MRI shows that imaging intensity increases with the increase of Fe concentration. The MR relaxation data and MRI results showed the potential of assynthesized NPs being used as T_2 MRI contrast agent.

4. Conclusions

Magnetic $\gamma \text{Fe}_2\text{O}_3$ NPs with mean size 6.5 nm were successfully synthesized by a sonochemical method. Polycondensation of APTS on γFe_2O_3 NPs led to the formation of APTS- γFe_2O_3 beads. These beads were modified with succinic anhydride to obtain CARB- γ Fe₂O₃ beads. The size of the beads was evaluated by TEM, which returned a mean size of 12 nm. The DLS results showed that the beads were aggregated and have a hydrodynamic size of 490 nm. The CARB- γ Fe₂O₃ and APTS- γ Fe₂O₃ beads had isoelectric points at pH of 3.76 and 6.41, respectively. The FTIR studies showed characteristic bands which demonstrated the presence of the amino and silane groups, at $870\,\mathrm{cm}^{-1}$ and $1352\,\mathrm{cm}^{-1}$, respectively, as well as carboxylate groups, at $1648\,\mathrm{cm}^{-1}$ and $1425\,\mathrm{cm}^{-1}$. To prove the ability of magnetic beads to couple proteins, rabbit antibody was covalently immobilized on these chemically modified beads. Mössbauer spectroscopy and VSM measurements showed that a large fraction of the beads have superparamagnetic behavior within the VSM measuring time. The XRD and Mössbauer results showed that capping with APTS did not induce any phase change in the maghemite phase. Immobilization time of rabbit antibodies was 4 h at a concentration of 120 mg per gram of NPs. The MRI results suggest that magnetic beads indeed constitute an excellent T_2 contrast agent candidate.

Acknowledgments

Authors thank the financial support of the Brazilian agencies MCT/CNPq, CAPES and INCT in Nanobiotechnology. Morales M thanks CNPq for his fellowship.

ORCID iDs

A F R Rodriguez https://orcid.org/0000-0002-3034-183X

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